

A new probabilistic rule for drug–drug interaction prediction

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Abstract An innovative probabilistic rule is proposed to predict the clinical significance or clinical insignificance of DDI. This rule is coupled with a hierarchical Bayesian model approach to summarize substrate/inhibitor's PK models from multiple published resources. This approach incorporates between-subject and between-study variances into DDI prediction. Hence, it can predict both population-average and subject-specific AUCR. The clinically significant DDI, weak DDI, and clinically insignificant inhibitions are decided by the probabilities of predicted AUCR falling into three intervals, $(-\infty, 1.25)$, $(1.25, 2)$, and $(2, \infty)$. The main advantage of this probabilistic rule to predict clinical significance of DDI over the deterministic rule is that the probabilistic rule considers the sample variability, and the decision is independent of sampling variation; while deterministic rule based decision will vary from sample to sample. The probabilistic rule proposed in this paper is best suited for the situation when in vivo PK studies and models are available for both the inhibitor and substrate. An early decision on clinically

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significant or clinically insignificant inhibition can avoid additional DDI studies. Ketoconazole and midazolam are used as an interaction pair to illustrate our idea. AUCR predictions incorporating between-subject variability always have greater variances than population-average AUCR predictions. A clinically insignificant AUCR at population-average level is not necessarily true when considering between-subject variability. Additional simulation studies suggest that predicted AUCRs highly depend on the interaction constant K_i and dose combinations.

Keywords Area under the concentration curve ratio (AUCR) · Bayesian model · Drug–drug interaction (DDI) · Pharmacokinetics · Prediction

Introduction

Drug–drug interactions (DDI) have become a significant concern for both pharmaceutical industries and FDA, since being exemplified by the interaction of ketoconazole and terfenadine, which caused potentially life-threatening ventricular arrhythmias [1], and the interaction between sorivudine and fluorouracil which resulted in fatal toxicity [2, 3]. The possible sites of DDI and static mechanistic models which can predict the change of pharmacokinetic (PK) profiles include (1) gastrointestinal absorption, (2) plasma and/or tissue protein binding, (3) carrier-mediated transport across plasma membranes, and (4) metabolism [4, 5]. Recently, the static metabolic DDI mechanism was integrated with PK models to predict the effects of dose staggering on DDIs [6]. The success of this approach has shown great potential in predicting *in vivo* DDI based on either *in vitro* or *in vivo* PK data. Both FDA and pharmaceutical industry have recognized the importance of early DDI detection, in which early negative findings can eliminate the need for later clinical investigations. FDA has recently issued a draft Guidance for Industry on Drug Interaction Studies (<http://www.fda.gov/cder/guidance/6695dft.pdf>) discussing study design, data analysis, and implications for dosing and labeling.

The extent of an *in vivo* DDI is measured by the ratio of the area under the substrate concentration–time curve (AUC) in the presence of inhibitor to the substrate’s AUC in the absence of an inhibitor (AUCR). The current rule proposed by FDA suggests that an AUCR greater than 2 is a clinically significant DDI, and an AUCR less than 1.25 is considered clinically insignificant. This rule has been implemented in literature of model-based DDI predictions [6, 7]. However, stochastic features of data from an individual drug’s PK study, PK models, and their parameters are not fully considered. To fulfill this imminent need, a probabilistic decision rule is proposed to facilitate DDI prediction. This probabilistic decision is built upon our Bayesian hierarchical PK model on individual drug’s PK data [8, 9]. The DDI can be predicted at either a subject-specific level, or a population-average level. This paper utilizes a previously reported Bayesian model predicting the *in vivo* effect of the potent CYP3A inhibitor ketoconazole (KETO) on the pharmacokinetics of midazolam (MDZ) [8, 9] to illustrate this novel probabilistic DDI prediction methodology. MDZ is a highly selective CYP3A substrate *in vivo* that is not dependent on membrane transporters for intracellular access [10].

The KETO/MDZ pair is employed as an inhibitor-substrate example to illustrate our model based DDI prediction.

Methods

KETO and MDZ PK models

Development of the KETO and MDZ interaction model has previously been described in detail [8, 9]. PK of both drugs were fit to a two-compartment model with occurring from the central compartment and systemic clearance assumed to be equivalent to hepatic clearance. Orally administered KETO was absorbed into the central circulation through a first-order process with no lag time. MDZ was administered to the systemic compartment by intravenous bolus. When KETO and MDZ are administrated separately, PK models (1) and (2), describe the plasma concentration time course, respectively, and these differential equations can be independently solved.

$$\begin{aligned} \frac{dA_{1I}}{dt} &= F_I \times Dose \times ka_I \times e^{-ka_I \times t} - CL_I \times \frac{A_{1I}}{V_{1I}} + \left(-\frac{A_{1I}}{V_{1I}} + \frac{A_{2I}}{V_{2I}} \right) \times CL_{12I}, \\ \frac{dA_{2I}}{dt} &= \left(\frac{A_{1I}}{V_{1I}} - \frac{A_{2I}}{V_{2I}} \right) \times CL_{12I}, \quad (A_{1I}, A_{2I})|_{t=0} = (0, 0), \end{aligned} \tag{1}$$

where subscript *I* indicates the inhibitor, KETO; the initial amount of KETO in two compartments $(A_{1I}, A_{2I})|_{t=0} = (0, 0)$; F_I is the bioavailability which is assumed to be known, 0.7 [11]; ka_I is the absorption rate constant; (V_{1I}, V_{2I}) are volumes of distribution in systemic and peripheral compartments, respectively; CL_{12I} is the between-compartment rate constant; CL_I is the hepatic (systemic) clearance, which is described by the well-stirred model $CL_I = Q_h \times CL_{int,I} / (Q_h + CL_{int,I})$, in which hepatic blood-flow, $Q_h = 80$ l/h [12] is known, and intrinsic hepatic clearance, $CL_{int,I} = fu_I \times V \max_I / (Km_I + fu_I \times A_{1I} / V_{1I})$, where $fu_I = 0.03$ [13].

$$\begin{aligned} \frac{dA_{1S}}{dt} &= -CL_S \times \frac{A_{1S}}{V_{1S}} + \left(-\frac{A_{1S}}{V_{1S}} + \frac{A_{2S}}{V_{2S}} \right) \times CL_{12S} \\ \frac{dA_{2S}}{dt} &= \left(\frac{A_{1S}}{V_{1S}} - \frac{A_{2S}}{V_{2S}} \right) \times CL_{12S}, \quad (A_{1S}, A_{2S})|_{t=0} = (Dose, 0) \end{aligned} \tag{2}$$

where subscript *S* represents substrate MDZ; (V_{1S}, V_{2S}) are volumes of distribution in systemic and peripheral compartments, respectively; CL_{12S} is the inter-compartment rate constant; CL_S is the hepatic (systemic) clearance, which follows a well-stirred model $CL_S = Q_h \times CL_{int,S} / (Q_h + CL_{int,S})$, and intrinsic clearance $CL_{int,S} = fu_S \times V \max_S / (Km_S + fu_S \times A_{1S} / V_{1S})$, in which $Km_S = 2.11$ and $fu_S = 0.04$, and the amount of drug in blood is transformed to plasma by multiplying 0.86. When the drugs are administrated simultaneously, KETO competitively inhibits the clearance of MDZ such that

$$CL_{\text{int},S} = \frac{fu_S \times V \max_S}{Km_S \times \left(1 + \frac{fu_l \times A1_l}{MW_l \times K_i \times V1_l}\right) + fu_S \times \frac{A1_S}{V1_S}} \quad (3)$$

A range of inhibition constants, $K_i = 0.18$ to 0.0037 , as set forth in the FDA's Guidance was tested (<http://www.fda.gov/cber/gdlns/interaction.pdf>). This model assumes that the clearance of KETO is not affected by MDZ administration. In addition, KETO has no effect on protein binding or disposition of MDZ other than altering its apparent K_m . The concentration of drug at the enzyme site is assumed to be equivalent to the plasma concentration.

A common criterion to evaluate the extent of interaction is the AUC ratio ($AUCR$) of substrate after and before inhibitor administration.

$$AUCR = \frac{AUC_{S,W}}{AUC_{S,W0}} \quad (4)$$

where, $AUC_{S,W}$ is the substrate AUC in the presence inhibitor and $AUC_{S,W0}$ is its AUC without inhibitor. AUC is estimated via the trapezoidal rule with extrapolation to infinity [14].

A hierarchical Bayesian meta-analysis model for published sample mean KETO and MDZ data sets

Published data (Table 1) are available in the form of sample average plasma drug concentration and its standard deviation [8, 9]. A hierarchical Bayesian meta-analysis model was developed to reconstruct a drug PK model from these published data. More details are illustrated in the Appendix. The following models from (5) to (8) are a brief summary,

Sample mean PK model

$$p(\bar{y}_{\bullet,jkh} | \beta_k, \Sigma, \Omega, \sigma_0^2) \sim N\left(f(\beta_k, t_{jkh}), \frac{F_{jkh}^T \Sigma F_{jkh} + \sigma_0^2}{n_{kh}}\right) \quad (5)$$

Sample variance model

$$\frac{(n_{kh} - 1)}{F_{jkh}^T \Sigma F_{jkh} + \sigma_0^2} s_{jkh}^2 \sim \chi_{n_{kh}-1}^2 \quad (6)$$

Study-specific PK parameter model:

$$p(\beta_k | \Omega) \sim N(\beta, \Omega), \quad (7)$$

Prior Distributions:

$$p(\beta) = U(0, 10^4), \quad p(\sigma_l^2) = U(0.01^2, 2^2), \quad l = 1, \dots, q. \quad (8)$$

where, $F_{jkh} = \partial f / \partial \beta_k^T$.

In this hierarchical model, $f(\beta_k, t_{jkh})$ denotes the predicted sample average log-transformed drug concentration at j th time point from phase h of study k . The sample mean data $\bar{y}_{\bullet,jkh}$ provides information about study specific PK parameters β_k

Table 1 Published KETO and MDZ data sets

Sources	Dose (mg)	Sample size per subject (time frame)	Size (M/F)	Meal
<i>KETO</i>				
[24]	200 capsule	5 (1–24 h)	3 (N/A)	Fasting
	200 solution	5 (1–24 h)	3 (N/A)	Fasting
	100,200,400 tablet	8 (0.5–48 h)	12 (N/A)	Meal
	200 solution	8 (0.5–48 h)	12 (N/A)	Meal
[25]	200, 400 tablet	14 (0.5–48 h)	28–44 6(6/0)	Meal
[26]	200 tablet, 7(0–24 h)	10 (0.5–8 h)	8 (8/0)	Fasting
[27]	200, 400, 600	13 (0.5, 32 h)	8 (3/5)	Meal
	800, tablet		(20–31)	
[28]	200 solution suspension, tablet	12 (0.5–48 h)	24 (24/0)	Fasting
	200, 400, 800 solution	12 (0.5–48 h)	12 (24/0)	Fasting
Novopharm Ltd	200 tablet	17 (1/4–24 h)	39 (39/0)	Fasting
(FDA, 1999)	200 tablet	17 (1/4–24)	23 (24/0)	Meal
TEVA Pharm.	200 tablet	15 (1/3–48)	24 (24/0)	Fasting
(FDA, 1999)	200 tablet	15 (1/3–48)	17 (17/0)	Meal
<i>MDZ</i>				
[29]	2 IV fusion	27 (1/2–6 h)	12 (6/6)	Fasting
[10]	2 IV	12 (1/4–8 h)	9 (6/3)	Fasting

and study to study variation parameter Σ . The standard deviation data s_{jkh}^2 provides information about subject level heterogeneity parameter Ω and technical variance, σ_0^2 . Variance components $\sigma_l^2, l = 1, \dots, q$, denote all the variance parameters. The estimation procedure is implemented with a Monte Carlo Markov chain process [8, 9], and is illustrated in the appendix. In particular, $\beta = (V1_S, V2_S, Vmax_S, Km_S, CL12_S)^T$ for MDZ, and $\beta = (V1_I, V2_I, Vmax_I, Km_I, CL12_I, ka_I)^T$ for KETO. The posterior 95% creditable intervals for population average PK parameters are summarized in Table 2.

Population average DDI prediction

Denote $AUCR_{pop}(\beta, K_i)$ as the population average DDI, where β are PK parameters from KETO and MDZ. Based on posterior distributions of PK parameters from the mean-variance model, we are able to obtain a predictive distribution of $AUCR_{pop}$ at the population-average level.

$$p[AUCR_{pop}(\beta, K_i) | \bar{Y}_\bullet, S] = \int p[AUCR(\beta, K_i) | \beta] p(\beta | \bar{Y}_\bullet, S) d\beta \tag{9}$$

This distribution can be sampled by $\{AUCR_{pop}^{(u)} = AUCR(\beta^{(u)}, K_i)\}_{u=1, \dots, U}$, where $\{\beta^{(u)}\}_{u=1, \dots, U}$ are their posterior draws. A sample size of $U = 1000$ is sufficiently large.

Table 2 PK parameters estimate for KETO and MDZ

KETO			MDZ		
Parameter	Est.	95% CI	Parameter	Est.	95% CI
$V1_I$	20.1	(0.84, 1.17)	$V1_S$	67.05	(0.73, 1.59)
$V2_I$	32.2	(0.56, 1.85)	$V2_S$	45.08	(0.65, 1.55)
$Vmax_I$	21.0	(0.83, 1.17)	$Vmax_S$	4284	(0.63, 1.43)
Km_I	0.48	(0.97, 1.06)	Km_S	2.11	(0.60, 1.80)
$CL12_I$	2.25	(0.54, 1.78)	$CL12_S$	42.9	(0.56, 1.60)
$ka_{I, TM}$	0.45	(0.78, 1.40)	$ka_{S, SL}$	1.86	(0.44, 2.29)
$ka_{I, TF}$	0.70	(0.78, 1.42)	$ka_{S, T}$	0.69	(0.09, 4.02)
$ka_{I, SPF}$	1.79	(0.76, 1.41)	$Fa_{S, SL}$	0.46	(0.55, 1.70)
$ka_{I, SLM}$	0.75	(0.74, 1.41)	$Fa_{S, T}$	0.24	(0.38, 2.13)
$ka_{I, SLF}$	2.18	(0.74, 1.44)	ω_{F_S}	0.29	(0.26, 2.23)
ω_{V1_I}	0.14	(0.40, 1.94)	ω_{V1_S}	0.39	(0.29, 1.57)
ω_{V2_I}	0.64	(0.43, 1.68)	ω_{V2_S}	0.43	(0.31, 1.66)
ω_{Vmax_I}	0.15	(0.52, 1.72)	ω_{Vmax_S}	0.36	(0.37, 1.44)
ω_{CL12_I}	0.72	(0.59, 1.74)	ω_{CL12_S}	0.43	(0.36, 1.58)
ω_{ka_I}	0.38	(0.47, 1.76)	ω_{ka_S}	0.36	(0.28, 2.28)

Subject-specific DDI prediction

The subject-specific DDI is defined as $AUCR_{subj}(\beta_{mk}, k_i)$ with a posterior distribution of

$$\begin{aligned}
 & p[AUCR(\beta_{mk}, K_i) | \bar{Y}_\bullet, S] \\
 &= \int p[AUCR(\beta_{mk}, K_i) | \beta_{mk}] p(\beta_{mk} | \beta_k, \Sigma) p(\beta_k | \beta, \Omega) p(\beta | \bar{Y}_\bullet, S) \\
 & \quad \times p(\Omega | \bar{Y}_\bullet, S) p(\Sigma | \bar{Y}_\bullet, S) d\beta d\beta_k d\Omega d\Sigma,
 \end{aligned} \quad (10)$$

This distribution can be sampled by

$$\left\{ AUCR_{subj}^{(u)} \sim AUCR\left(\beta^{(u)}, \beta_k^{(u)}, \beta_{mk}^{(u)}, \Omega^{(u)} \Sigma^{(u)}, K_i\right) \right\}_{u=1, \dots, U}, \quad (11)$$

where $\{\beta^{(u)}, \beta_k^{(u)}, \beta_{mk}^{(u)}, \Omega^{(u)}, \Sigma^{(u)}\}_{u=1, \dots, U}$ are their posterior draws. A sample size of $U = 1000$ is sufficiently large. In this context, subject-specific DDI prediction means that random samples are drawn from the between-subject distributions that don't correspond to real subjects. It doesn't mean subject-specific predictions related to specific datasets, especially in the Bayesian context.

Both population-average and subject-specific DDI predictions are improvements over the deterministic approach [6], in which β were chosen as a set of fixed numbers (i.e. their estimates), and their estimation error and between-study/subject variation information were totally ignored.

Probabilistic DDI prediction rule

The current rule proposed by the FDA suggests that an AUCR greater than 2 is considered to be a clinically significant inhibition, an AUCR less than 1.25 is treated as clinically insignificant, and any AUCR falling into between 1.25 and 2 is claimed as a weak inhibition. By taking account of the uncertainty of PK parameter estimates, and their between subject and study variations, a probabilistic rule is proposed: if 90% of predicted AUCR > 2, the inhibition is concluded as statistically significant at the clinically significant level; if 90% of predicted AUCR is below 1.25, the inhibition is statistically significant at the non-clinical level; otherwise, the inhibitor is concluded to be weak. In particular, the population average and subject-specific probabilities are estimated as,

$$\begin{aligned} \hat{\Pr}(AUCR_{pop} \in E) &= \frac{\sum_{u=1}^U 1\{AUCR_{pop}^{(u)} \in E\}}{U}, \\ \hat{\Pr}(AUCR_{subj} \in E) &= \frac{\sum_{u=1}^U 1\{AUCR_{subj}^{(u)} \in E\}}{U}, \end{aligned} \tag{12}$$

where $E = (-\infty, 12.5), (1.25, 2), (2, \infty)$.

KETO/MDZ inhibition predictions and sensitivity analysis

The dose combination of KETO/MDZ is chosen as 200/2 mg and 800/10 mg. Following the FDA’s guideline, K_i is tested on two ends of the interval (0.0037, 0.18). In addition, the time interval between the administration of KETO and MDZ are tested between -12 and 12 h. In addition, the effect of food and dosage formulation of KETO on the AUCR of MDZ was examined.

Results

Population-average DDI prediction

Given a 200/2 mg KETO/MDZ dose combination, the population average AUCR is predicted from 1.21 \times/\div 1.013 (geometric mean \times/\div (1 + CV)) to 3.02 \times/\div 1.11 for $K_i = (0.18, 0.0037)$, respectively (Table 3). Its probabilities in three intervals are, (0.98, 0.02, 0.0) and (0.0, 0.0, 1.0), respectively (Fig. 1a, b). Therefore, the

Table 3 Population average DDI prediction

K_i	KETO (mg)/MDZ (mg)	
	200/2	800/10
0.18	1.21 \times/\div 1.013	1.78 \times/\div 1.027
0.0037	3.02 \times/\div 1.11	3.93 \times/\div 1.14

Geometric mean \times/\div (1 + CV) of the predicted AUCR

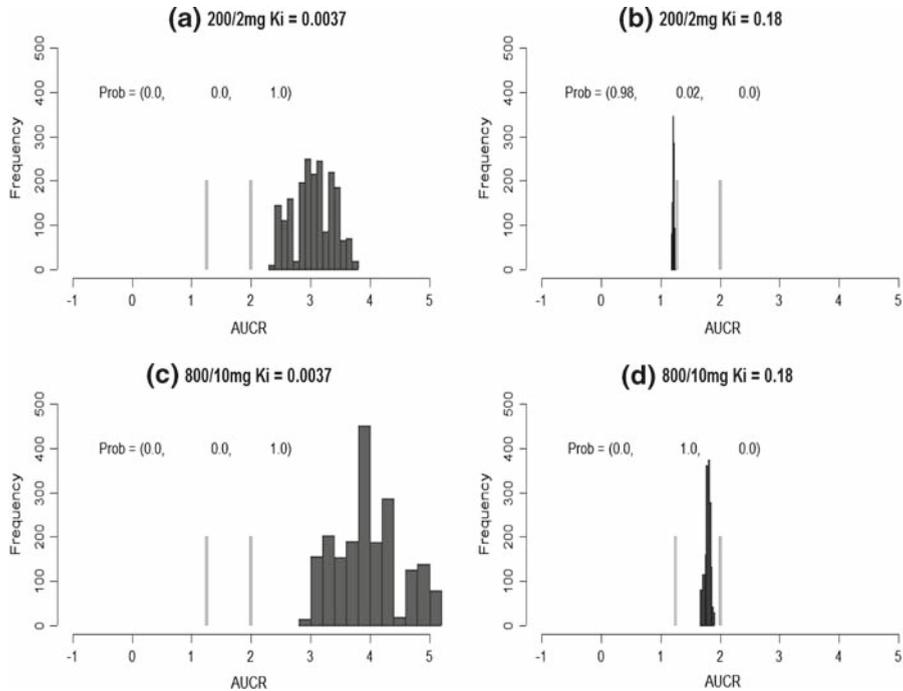


Fig. 1 Population average DDI prediction. The *gray bars* cut the axis into three intervals, $(-\infty, 1.25)$, $(1.25, 2)$, $(2, \infty)$. The probabilities on the top represent the probabilities falling into these intervals. **a–d** The predicted population average DDI at various dose combinations and K_i

conclusion of the inhibition can be either clinically or non-clinically significant, which depends on K_i .

With a much higher dose combination, 800/10 mg, a K_i of 0.18 leads to a predicted $AUCR_{pop} = 1.78 \times / \div 1.027$ (Table 3). Its probabilities in three intervals are (0.0, 1.0, 0.0) (Fig. 2d), and the inhibition is concluded as a weak one. On the other hand, for a much smaller K_i , 0.0037, $AUCR_{pop}$ is predicted as $3.93 \times / \div 1.14$ with probabilities, (0.0, 0.0, 1.0) (Fig. 2c), and inhibition is concluded to be both statistically and clinically significant.

Subject-specific DDI prediction

Providing a 200/2 mg KETO/MDZ dose combination, the predicted $AUCR_{subj}$ based on between-subject variation is from $1.19 \times / \div 1.084$ to $2.95 \times / \div 1.26$ for K_i of 0.18 and 0.0037, respectively (Table 4). Its probabilities in three intervals are (0.75, 0.25, 0.0) and (0.0, 0.06, 0.94), respectively (Fig. 2a, b). Therefore, $K_i = 0.18$ will lead to a weak DDI conclusion, and $K_i = 0.0037$ will lead to a statistically and clinically significant DDI. Given a much higher dose combination, 800/10 mg, a K_i of 0.18 leads to a predicted $AUCR_{subj} = 1.69 \times / \div 1.15$ (Table 4). Its probabilities in three intervals are (0.01, 0.85, 0.14) (Fig. 3d), and the inhibition is concluded as a

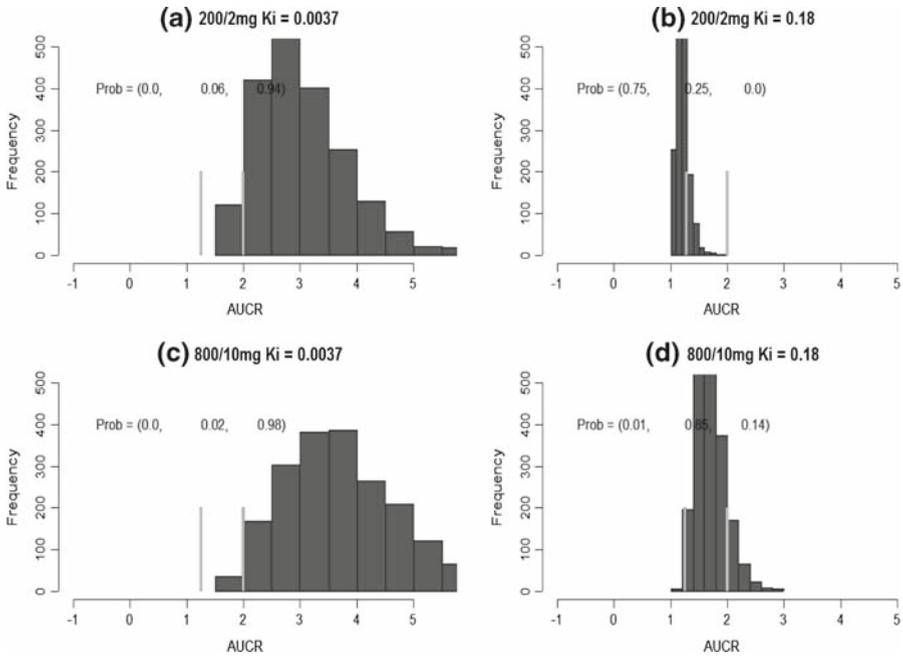


Fig. 2 Subject-specific DDI prediction. The gray bars cut the axis into three intervals, $(-\infty, 1.25)$, $(1.25, 2)$, $(2, \infty)$. The probabilities on the top represent the probabilities falling into these intervals. **a–d** The predicted subject-specific DDI at various dose combinations and K_i

Table 4 Subject-specific DDI prediction

K_i	KETO (mg)/MDZ (mg)	
	200/2	800/10
0.18	1.19 \times/\div 1.084	1.69 \times/\div 1.15
0.0037	2.95 \times/\div 1.26	3.61 \times/\div 1.28

Geometric mean \times/\div $(1 + CV)$ of the predicted AUCR

weak one. On the other hand, for a much smaller K_i , 0.0037, $AUCR_{subj}$ is predicted as 3.61 \times/\div 1.28 with probabilities, (0.0, 0.02, 0.98) (Fig. 3c), and inhibition is concluded both statistically and clinically significant.

The effect of dosing interval on KETO/MDZ interaction

Administration of the KETO PO dose (800 mg) was simulated from 12 h before to 12 h after the MDZ IV dose (10 mg), with K_i set at 0.0037. According to the previous analysis, simultaneous KETO/MDZ interaction showed the highest interaction based on this dose and K_i combination. Figure 3a presents the relationship between the time between KETO and MDZ doses and predicted subject-specific level AUCR. The solid line is $AUCR_{subj}$, and the dashed lines are its

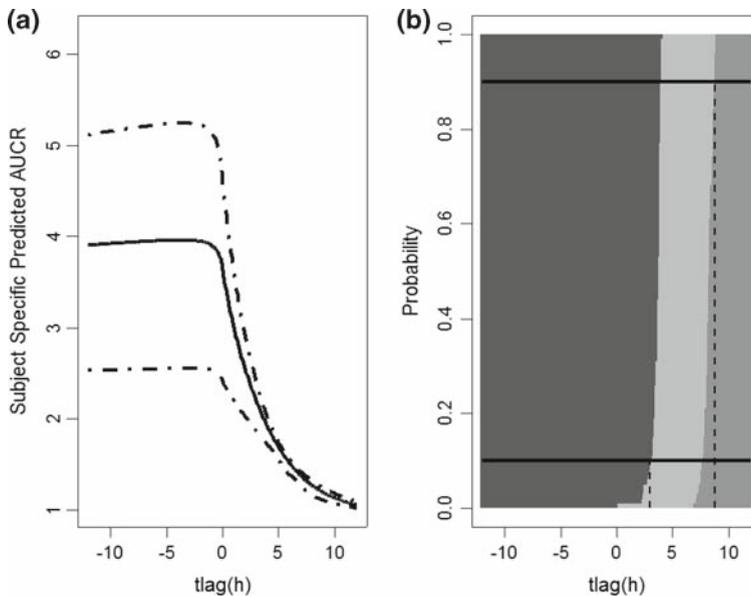


Fig. 3 Effects of dosage separation on DDI when KETO(PO)/MDZ(IV) combination is 800/10 mg and $K_i = 0.0037$. **a** The mean and 90% credit intervals for AUCR predicted based on between-subject variability across the interval from -12 to 12 h. *Negative values* indicate that KETO is administered before MDZ, and positive that MDZ administered prior to KETO. **b** The *dark gray* represents $\Pr\{AUCR_{subj} > 2\}$, the *light gray* represents $\Pr\{1.25 < AUCR_{subj} < 2\}$, the *gray* represents $\Pr\{AUCR_{subj} < 1.25\}$. The *top black solid horizontal line* represents the probability = 0.9, and it crosses the red region when the interval between administration is 8.8, indicating that if PO KETO is administered 8.8 h after MDZ IV or later, the effect on AUCR will be clinically insignificant with probability larger than 90%. The *black solid line at the bottom* represents probability = 0.1, and it crosses the blue region when the time interval between dosage of interacting drugs is 3.0, meaning that if PO KETO is administered within 3 h after MDZ IV, the inhibition will be clinically significant with probability larger than 90%. Otherwise, their DDI will be a weak interaction

95% credit intervals. The maximum $AUCR_{subj}$ happens when KETO is administered about 4.5 h before MDZ, $AUCR_{subj} = 4.02 \times / \div 1.31$. At the mean level, this is 11% greater than the $AUCR_{subj}$ when the drugs are administered simultaneously, $3.61 \times / \div 1.28$.

If KETO is administered after MDZ, its inhibition effect is quickly diminished. In order to tell the probabilities of $AUCR_{subj}$ falling into three DDI intervals, they are displayed in a heatmap (Fig. 3b). The blue represents $\Pr\{AUCR_{subj} > 2\}$, the green represents $\Pr\{1.25 < AUCR_{subj} < 2\}$, the red represents $\Pr\{AUCR_{subj} < 1.25\}$, with these probabilities represented across the differences in dosing times. The top black solid horizontal line represents the probability = 0.9, and it crosses the red region when KETO is administered 8.8 h after MDZ. Thus, if PO KETO is administered more than 8.8 h after MDZ IV, their inhibition will be clinically insignificant with probability larger than 90%. The black solid line at the bottom of Fig. 3 represents a probability = 0.1 and intersects the blue region at +3.0 h, indicating that if PO KETO is administered before or within 3 h after MDZ IV, it will cause a clinically

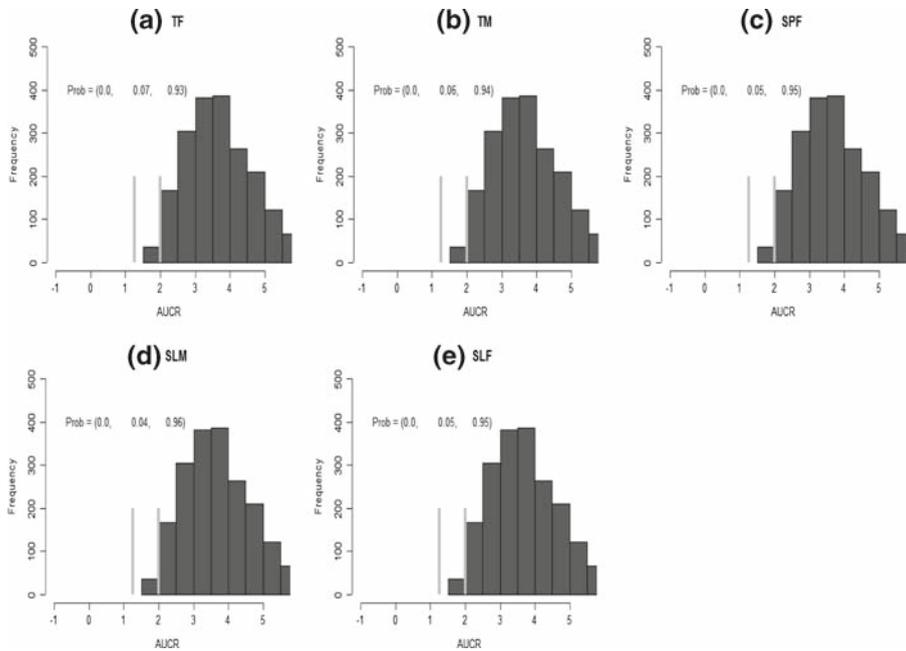


Fig. 4 The effect of KETO administration route on AUCR. Predictions incorporated individual subject variability. The notations (TF, TM, SPF, SLM, SLF) represent tablet fasting (a), tablet meal (b), suspension fasting (c), solution meal (d), and solution fasting (e), respectively. The KETO(PO)/MDZ(IV) combination is 800/10 mg and $K_i = 0.0037$

significant reduction in MDZ clearance with probability greater than 90%. Otherwise, their DDI will be a weak interaction.

The effect of KETO formulation and food on subject specific AUCR prediction

Published KETO PK studies used to develop the model [8, 9] utilized various KETO formulations and conditions: tablet fasting (TF), tablet with a meal (TM), suspension fasting (SPF), solution with a meal (SLM), and solution fasting (SLF), respectively. The corresponding k_a posterior distributions were estimated from published sample mean data. The effects of food and formulation on the predicted $AUCR_{subj}$ are displayed in Fig. 4. When KETO/MDZ dose combination is 800/10 mg and $K_i = 0.0037$, they all have similar distributions, and the probabilities in three DDI intervals are very similar.

Discussion

An innovative probabilistic rule is proposed to predict the clinical significance or clinical insignificance of DDI. A KETO/MDZ inhibition combination is used as an example. This rule can be applied to predictions of both population-average and

subject-specific level AUCR's to determine the extent of a DDI. As shown, $AUCR_{subj}$ prediction always exhibit larger variances than the corresponding $AUCR_{pop}$. Hence, a clinically insignificant $AUCR_{pop}$ is not necessarily true when considering between-subject variability. For example, under the 200/2 mg KETO/MDZ dose combination and a $K_i = 0.18$, the population-average DDI claim an insignificant KETO/MDZ interaction (Fig. 1b). On the other hand, its subject-specific level prediction is concluded as a weak DDI (Fig. 2b).

It is very clear that AUCR highly depends on the K_i and dose combination chosen. Simulations were run with K_i set at 0.0037 or 0.18 μM , the values set forth in the FDA Guidance (<http://www.fda.gov/cder/guidance/6695dft.pdf>). This nearly 50-fold range in the in vitro K_i values can greatly impact the conclusion of DDI significance. This variability may arise from different buffer conditions, the enzyme source, and the concentration of substrate and inhibitor studied. Hepatocyte and microsomal studies may yield different results as hepatocytes require that the drug access an intact cell system [15]. Standardization and optimization of the in vitro assay to determine K_i is necessary to accurately predict DDI potential of a new compound. Similarly, the design of the clinical trial can influence the effect of the DDI. The trial should be designed to determine the “worst-case scenario,” i.e. doses of KETO and MDZ should be administered at a time when maximal inhibition is likely to occur. As shown in Fig. 4, KETO administered 4.5 h before MDZ would result in the maximal interaction.

The main advantage of probabilistic rule to predict clinical significance of DDI over the deterministic rule is that the probabilistic rule considers the sample variations, while deterministic rule does not. For example, for a dose combination 200/2 mg and $K_i = 0.18 \mu\text{M}$, predicted $AUCR_{subj}$ is $1.19 \times / \div 1.084$ and its probabilities in the three intervals are 0.75, 0.25, 0.0. Based on this, it is classified as a weak inhibitor. However, if it is judged under the deterministic rule, 75% of time it will be declared insignificant inhibition, and 25% of time it will claimed to be a weak inhibitor.

We utilized a hierarchical Bayesian meta-analysis model designed to summarize published sample mean and sample variance data [8, 9]. It is capable of recovering between subject and between study variances. Information from these recovered variances information became the foundation for the AUCR prediction at the subject level. On the other hand, if the data from original PK studies are available with PK parameters for each individual, many conventional Bayesian PK models can be applied [16–21].

There are several limitations in the MDZ/KETO model that we applied to illustrate our probabilistic rule. For instance, the current MDZ model (2) assumes that 100% of clearance is by hepatic CYP3A. However, approximately 10% of MDZ's clearance is through non-CYP3A mechanisms. Incorporating non-inhabitable elimination will reduce the extent of the DDI. These models also assume that the concentration of substrate (MDZ) and inhibitor (KETO) at the active site is equivalent to the concentration in the central compartment. A potentially higher active site concentration of KETO will lead to a larger AUCR. This paper only considers the inhibition of MDZ administered by IV route. A similar model for PO MDZ is more complex as it would need to incorporate information on inhibition of CYP3A in the intestine.

The model does not take any correlation between the PK of MDZ and KETO for an individual person into account. While we recognize that the CL of the two drugs may be related, e.g. to body weight or genotype, we do not currently have the information required to build this correlation into our model.

While we utilized our Bayesian MCMC model to estimate between-subject variability in PK parameters, the probabilistic rule proposed in this paper may be applied to any situation in which the individual PK models, incorporating variability, are available for both the inhibitor and substrate. It fits well with newly developed FDA guidelines for exploratory IND studies (<http://www.fda.gov/cder/guidance/6695dft.pdf>). This document highly recommends a PK study of an investigational drug at a very low dosing level and of a short duration. The purpose is to obtain this drug's PK, instead of investigating its pharmacologic effects. If this investigational drug is an inhibitor, its PK data and model may be incorporated with PK data that is available for many common substrates and the K_i values determined in vitro for the substrate-inhibitor combination. The interaction potential of this new agent can thus be predicted at both subject-specific and population-average levels. This same strategy can be applied to a new compound that is a substrate by nature, utilizing PK data for the enzyme inhibitor (e.g. KETO). If one is able to predict either a clinically significant or insignificant DDI with probability greater than 90%, no further in vivo DDI study may be required. Only when predicted as a weak DDI, a further in vivo DDI may be required to assess the clinical extent of the interaction. In these cases, utilizing the predictive PK interaction model may enhance the design of a trial to determine a DDI. As shown in Fig. 3, the time interval between administration of inhibitor and substrate may impact the AUCR.

If a drug's in vivo pharmacokinetics variability isn't available, they can be built up with data known for drugs in the same class, or information on enzyme variability (e.g. genetic variation), or variability seen in vitro (e.g. in hepatocytes obtained from different individuals). This bottom-up strategy is described in the literature [22]. The challenge of this approach is to establish and validate the equivalence between predicted DDI variability and clinical DDI variability.

The probabilistic decision rule presented here provides an alternative to the deterministic rule commonly utilized. This novel method takes into account stochastic variability in the determination of a clinically significant DDI. While DDI may be predicted using both population-average and subject-specific data, we recommend subject-specific DDI prediction since it contains more information on variation across the population.

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Appendix

Meta-analysis models for individual level data

When individual level data are available for each study, summarizing PK parameters from multiple sources by meta-analysis has been addressed by applying

Bayesian methods to construct a drug PK model from several clinical study data sets. (See, e.g. Wakefield and Rahman [20]). In general, the following set of models are used

- subject-specific PK model:

$$[y_{mjkh} | \beta_{mk}, z_{jkh}] \sim MVN[f(\beta_{mk}, z_{jkh}), \sigma_0^2], \quad (13)$$

- subject-specific PK parameter model in study k :

$$[\beta_{mk} | \beta_k, \Sigma] \sim MVN(\beta_k, \Sigma), \quad (14)$$

- study-specific PK parameter model:

$$(\beta_k | \beta, \Omega) \sim MVN(\beta, \Omega) \quad (15)$$

In (13), y_{mjkh} represents log-transformed drug concentration at time t_{jkh} for subject m in phase h of study k . Here we use a generic notation z_{jkh} to denote available data and constants for a study subject at time t_{jkh} . It includes dosage, dosing route, and fixed constants such as Q_h , F_l , Km_l , fu_l , MW_l , Km_s , fu_s , and time point t_{jkh} at which plasma concentration is measured. The mean value $f(\beta_{mk}, z_{jkh})$ is the predicted log-transformed drug concentration for subject m at j th time point from phase h of study k . In the case that y_{mjkh} is the KETO concentration observed from the first compartment, then $f(\beta_{mk}, z_{jkh}) = \log(A1_l/V1_l)$. The measurement error variation, σ_0^2 , is assumed equal across studies. The variance components Σ and Ω are for subject-specific and study-specific PK parameters.

However, published data are often available in the form of sample average plasma concentration. In other words, only $(\bar{y}_{\bullet jkh}, s_{jkh}^2)$, instead of y_{ijkh} are published. But model (13) obviously needs y_{mjkh} , and hence cannot be directly implemented to perform meta-analysis with summarized data. Reconstructing a drug PK model from $(\bar{y}_{\bullet jkh}, s_{jkh}^2)$ needs a new meta-analysis formulation and different Bayesian sampling algorithm.

Meta-analysis models with sample mean and standard deviation data

As individual data are not available, it is an unrealistic goal to estimate subject level PK parameters. The sample mean data $\bar{y}_{\bullet jkh}$ at most provide information about study specific PK parameters β_k and study to study variation parameters Ω . The sample variance data s_{jkh}^2 at most provide information about between-subject heterogeneity parameter Σ . As a result, models based on (13)–(15) are only suitable when working on subject level data. When only sample mean and sample variance data are available, they need to be modified to make estimation feasible. In other words, the models should not involve β_{mk} . A natural approach is to base estimation methods on marginalized likelihood where β_{mk} is integrated out. However, as no analytic form is available for $f(\beta_{mk}, z_{jkh})$, direct integration is not feasible. The alternative we take is

to first derive an approximation for $f(\beta_{mk}, z_{jkh})$ and then marginalize. Specifically, we adapt as follows.

By Taylor expansion at β_k , $f(\beta_{mk}, z_{jkh})$ can be approximated as

$$f(\beta_{mk}, z_{jkh}) \approx f(\beta_k, z_{jkh}) + \left(\frac{\partial f}{\partial \beta_{mk}} \Big|_{\beta_{mk}=\beta_k} \right)^T (\beta_{mk} - \beta_k). \tag{16}$$

Denote $F_{jkh} = \frac{\partial f}{\partial \beta_{mk}} \Big|_{\beta_{mk}=\beta_k}$. Instead of individual level PK model (16), we assume the following *approximated* model $[y_{mjkh} | \beta_{mk}, \beta_k, \sigma_0^2, z_{jkh}] \sim N(f(\beta_k, z_{jkh}) + F_{jkh}^T (\beta_{mk} - \beta_k), \sigma_0^2)$. Now by integrating out β_{mk} using the conditional distribution of β_{mk} given β_k , we have

$$[y_{mjkh} | \beta_k, z_{jkh}, \Sigma, \sigma_0^2] \sim N(f(\beta_k, z_{jkh}), F_{jkh}^T \Sigma F_{jkh} + \sigma_0^2). \tag{17}$$

As a result,

$$[\bar{y}_{\bullet jkh} | \beta_k, z_{jkh}, \Sigma, \sigma_0^2] \sim N\left(f(\beta_k, z_{jkh}), \frac{F_{jkh}^T \Sigma F_{jkh} + \sigma_0^2}{n_{kh}}\right) \tag{18}$$

To obtain the approximate distribution for sample variance, $s_{jkh}^2 = \sum_{i=1}^{n_{kh}} (y_{ijkh} - \bar{y}_{\bullet jkh})^2 / (n_{kh} - 1)$, we use the known fact the normalized sample variance of m i.i.d. normal variables has a Chi-square distribution with degree of freedom $m - 1$. From the approximate model (18), we immediately obtain

$$\frac{\sum_{i=1}^{n_{kh}} (y_{ijkh} - \bar{y}_{\bullet jkh})^2}{F_{jkh}^T \Sigma F_{jkh} + \sigma_0^2} \sim \chi_{n_{kh}-1}^2, \text{ or equivalently, } \frac{(n_{kh} - 1)}{F_{jkh}^T \Sigma F_{jkh} + \sigma_0^2} s_{jkh}^2 \sim \chi_{n_{kh}-1}^2 \tag{19}$$

Notice that (18) and (19) depend only on β_k , Σ , and σ_0^2 . Hence estimation of these parameters is feasible with mean and standard deviation data. Our estimation will be based on the following hierarchical models.

- Sample mean PK model

$$[\bar{y}_{\bullet jkh} | \beta_k, z_{jkh}, \Sigma, \sigma_0^2] \sim N\left(f(\beta_k, z_{jkh}), \frac{F_{jkh}^T \Sigma F_{jkh} + \sigma_0^2}{n_{kh}}\right) \tag{20}$$

- Sample variance PK model

$$\frac{(n_{kh} - 1)}{F_{jkh}^T \Sigma F_{jkh} + \sigma_0^2} s_{jkh}^2 \sim \chi_{n_{kh}-1}^2 \tag{21}$$

- Study-specific PK parameter model:

$$[\beta_k | \beta, \Omega] \sim MVN(\beta, \Omega) \tag{22}$$

Many times, a main purpose of determining variability is to identify individuals at risk. However as our model is based on summarized data, no individual

information is available. All we can do is to quantify variance for a given population. Of course if individual data are available, subject covariates can be used in explaining variability using individual level models.

Prior specification and posterior distributions

$$\begin{aligned}
 p(\beta) &= U(0, 10^4) \\
 p(\sigma_l^2) &= U(a, b) \Leftrightarrow p(\sigma_l^{-2}) = \frac{(\sigma_l^{-2})^{-2}}{(b-a)}, \quad l = 0, 1, \dots, q; \\
 p(\omega_l^2) &= U(a, b) \Leftrightarrow p(\omega_l^{-2}) = \frac{(\omega_l^{-2})^{-2}}{(b-a)}, \quad l = 1, \dots, q.
 \end{aligned}
 \tag{23}$$

Variance components all follow a uniform prior because practically they rarely exceed the bound $(a, b) = (0.01^2, 2^2)$. Let $\bar{Y}_\bullet = \{\bar{y}_{\bullet jkh}; j = 1, \dots, T_{kh}; k = 1, \dots, K; h = 1, \dots, H_k\}$ be the sample mean data and $S = \{S_{jkh}^2; j = 1, \dots, T_{kh}; k = 1, \dots, K; h = 1, \dots, H_k\}$ the sample variance data. Then, the posterior probability distribution based on (20)–(22) and priors (23) is,

$$\begin{aligned}
 &p(\beta_1, \dots, \beta_K, \Sigma, \Omega, \sigma_0^2 | \bar{Y}_\bullet, S, z) \\
 &\propto \left\{ \prod_{k=1}^K \prod_{h=1}^{H_k} \prod_{j=1}^{T_{kh}} N \left(\bar{y}_{\bullet jkh} | f(\beta_k, t_{jkh}), \frac{F_{jkh}^T \Sigma F_{jkh} + \sigma_0^2}{n_{kh}} \right) \right\} \\
 &\times \left\{ \prod_{k=1}^K \prod_{h=1}^{H_k} \prod_{j=1}^{T_{kh}} \chi_{n_{kh}-1}^2 \left(\frac{(n_{kh} - 1) s_{jkh}^2}{F_{jkh}^T \Sigma F_{jkh} + \sigma_0^2} \right) \right\} \\
 &\times \left\{ \prod_{k=1}^K p(\beta_k | \beta, \Omega) \right\} \times p(\beta) \times p(\Sigma) \times p(\Omega) \times p(\sigma_0^2)
 \end{aligned}
 \tag{24}$$

The estimation procedure is implemented with a Monte Carlo Markov chain method. The posterior probability functions, $p(\beta | \bullet)$, $p(\beta_k | \bullet)$, $p(\sigma_0^{-2} | \bullet)$, $p(\sigma_l^{-2} | \bullet)$, and $p(\omega_l^{-2} | \bullet)$ are derived in the following.

$$p(\beta_k | \bullet) \propto \left\{ \prod_{h=1}^{H_k} \prod_{j=1}^{T_{kh}} N \left(f(\alpha, \beta_k, z_{jkh}), \frac{F_{jkh}^T \Sigma F_{jkh} + \sigma_{0k}^2}{n_k} \right) \right\} \times \left\{ \prod_{k=1}^K p(\beta_k | \beta, \Omega) \right\}
 \tag{25}$$

$$p(\beta_l | \bullet) \propto N \left(\left\{ \frac{1}{\tau_l^2} + \frac{K}{\omega_l^2} \right\}^{-1} \left\{ \frac{1}{\tau_l^2} \mu_l + \frac{K}{\omega_l^2} \bar{\beta}_{\bullet l} \right\}, \left\{ \frac{1}{\tau_l^2} + \frac{K}{\omega_l^2} \right\}^{-1} \right)
 \tag{26}$$

for $l = 1, \dots, q$; where $\bar{\beta}_{\bullet l} = \sum_{k=1}^K \beta_{kl}$ Variance components:

$$\Pr(\omega_l^2 | \bullet) \sim \text{Inv - Gamma} \left[\left(\frac{K}{2} - 1 \right), \left(\frac{\sum_{k=1}^k (\beta_{kl} - \beta_l)^2}{2} \right) \right] \times 1_{\omega_l^2}(0.01^2, 2^2)
 \tag{27}$$

where $1_{\omega_l^2}(0.01^2, 2^2)$ equals 1 when ω_l^2 is inside $(0.01^2, 2^2)$ and 0 otherwise.

$$\begin{aligned}
 p(\sigma_1^2|\bullet) &\propto \prod_{k=1}^K \prod_{h=1}^{H_k} \prod_{j=1}^{T_{kh}} \left(F_{jkh}^T F_{jkh} \sigma_1^2 + \sigma_0^2 \right)^{-\frac{n_{kh}}{2}+1} \\
 &\times \exp \left\{ -\frac{n_{kh} \{ \bar{y}_{\bullet jkh} - f(\alpha, \beta_k, z_{jkh}) \}^2 + \sum_{i=1}^{n_{kh}} (y_{ijkh} - \bar{y}_{\bullet jkh})^2}{2 \left(F_{jkh}^T F_{jkh} \sigma_1^2 + \sigma_0^2 \right)} \right\} \\
 &\times 1_{\sigma_1^2}(0.01^2, 2^2) \\
 p(\sigma_0^2|\bullet) &\propto \prod_{k=1}^K \prod_{h=1}^{H_k} \prod_{j=1}^{T_{kh}} \left(F_{jkh}^T F_{jkh} \sigma_1^2 + \sigma_0^2 \right)^{-\frac{n_{kh}}{2}+1} \\
 &\times \exp \left\{ -\frac{n_{kh} \{ \bar{y}_{\bullet jkh} - f(\alpha, \beta_k, z_{jkh}) \}^2 + \sum_{i=1}^{n_{kh}} (y_{ijkh} - \bar{y}_{\bullet jkh})^2}{2 \left(F_{jkh}^T F_{jkh} \sigma_1^2 + \sigma_0^2 \right)} \right\} \\
 &\times 1_{\sigma_0^2}(0.01^2, 2^2) \tag{29}
 \end{aligned}$$

Here $1_{\sigma_1^2}(0.01^2, 2^2)$ and $1_{\sigma_0^2}(0.01^2, 2^2)$ are similarly defined as $1_{\omega_i^2}(0.01^2, 2^2)$.

MCMC convergence

Samples are drawn through the Metropolis Hasting (MH) algorithm (Hastings et al. 1970). At each step, a random walk chain is used and the random perturbation is taken to mean normal with mean 0 and standard deviation of 10%. The mixing is well with such proposed density and the acceptance rate varies. For most of the study specific parameters β_k , the acceptance rates are close to 25%. Five independent chains were run simultaneously to determine the convergence with dispersed starting values on population parameters. It needed less than 4000 iterations for the estimated potential scale reduction criterion of Gelman and Rubin [23] to be less than 1.2. By visual inspection of trace plots, almost all chains start to mix well after 500 iterations. The final results are based on a single chain of 50,000 iterations after a burn-in of 10,000. Every tenth iteration after burn-in was extracted for summarizing results.

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