

Computational Modelling of Mechanics and Transport in Growing Tissue

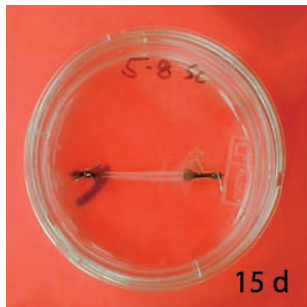
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University of Michigan

Eighth U.S. National Congress on Computational Mechanics

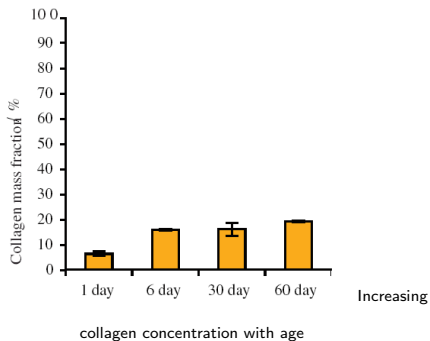
July 25th, 2005 – Austin, TX

Motivation and definition

Growth/Resorption – An addition or loss of mass

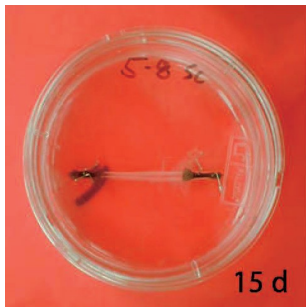


Engineered tendon constructs [Calve et al, 2004]

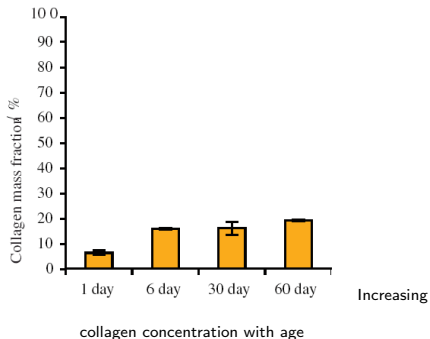


Motivation and definition

Growth/Resorption – An addition or loss of mass



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Open system with multiple species inter-converting and interacting

Modelling approach

Classical balance laws enhanced via fluxes and sources

- Solid – Collagen, proteoglycans, cells
- Extra cellular fluid
 - Undergoes transport relative to the solid phase
- Dissolved solutes (sugars, proteins, ...)
 - Undergo transport relative to fluid

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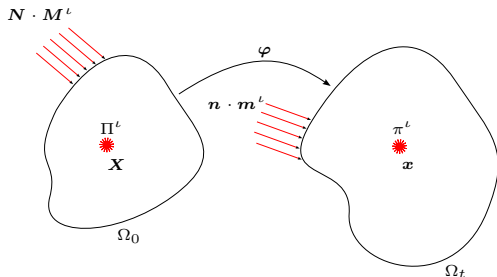
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Brief subset of related literature:

- Cowin and Hegedus [1976]
- Kuhl and Steinmann [2002]
- Sengers, Oomens and Baaijens [2004]
- *Garikipati et al. – Journal of the mechanics and physics of solids (52) 1595-1625 [2004]*

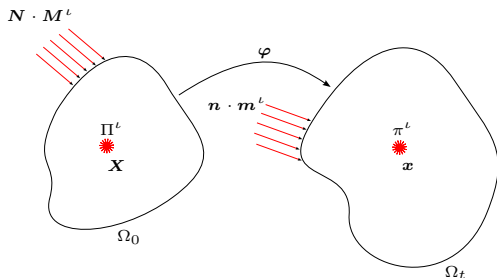
Balance of mass



ρ_0^l – Species concentration
 Π^l – Species production
 M^l – Species flux

- For a species:
$$\frac{\partial \rho_0^l}{\partial t} = \Pi^l - \nabla_X \cdot M^l$$
- Solid – No flux; No boundary conditions
- Fluid – No source; Concentration or flux boundary conditions
- Solute – Flux and source; Concentration boundary condition

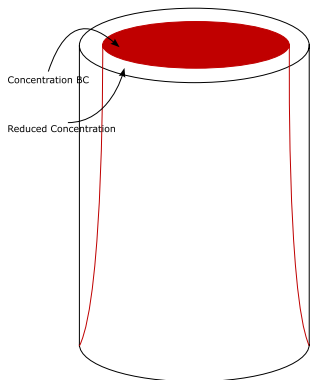
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Configuration and physical boundary conditions



Concentration BC

Reduced Concentration

Boundary condition specification

$$\frac{d\rho^i}{dt} + \rho^i \nabla_x \cdot \mathbf{v} = -\nabla_x \cdot \mathbf{m}^i + \pi^i$$

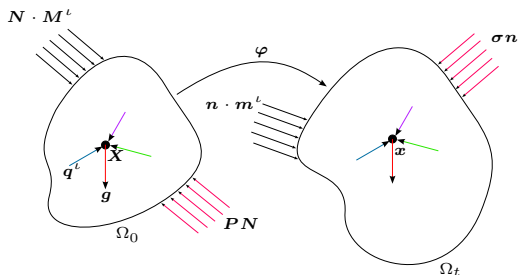
ρ^i – Current species concentration

π^i – Current species production

\mathbf{m}^i – Current species flux

\mathbf{v} – Solid velocity

Balance of momentum



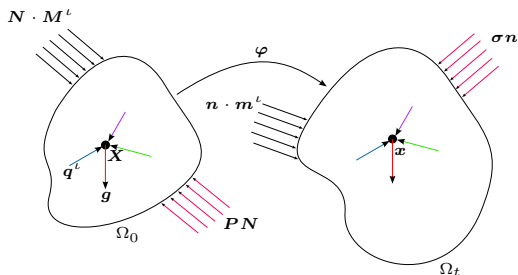
ρ_0^l – Species concentration
 V – Solid velocity
 V^l – Species relative velocity
 g – Body force
 q^l – Interaction force
 P^l – Partial stress

- For a species, velocity relative to the solid: $V^l = (1/\rho_0^l) F M^l$

$$\rho_0^l \frac{\partial}{\partial t} (V + V^l) = \rho_0^l (g + q^l) + \nabla_x \cdot P^l - (\nabla_x (V + V^l)) M^l$$

- Negligible contribution to mechanics from dissolved solutes

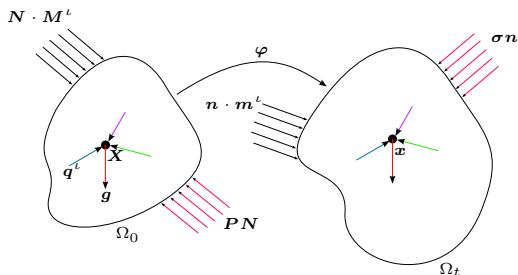
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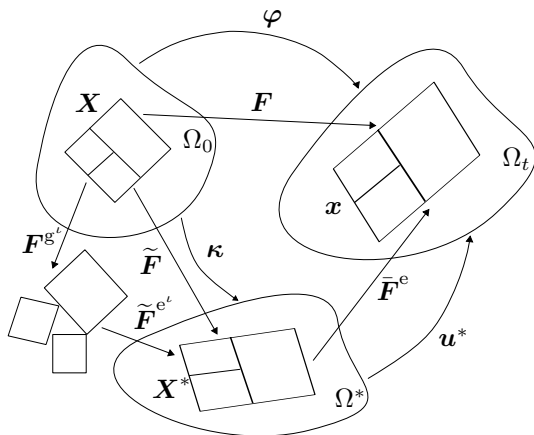
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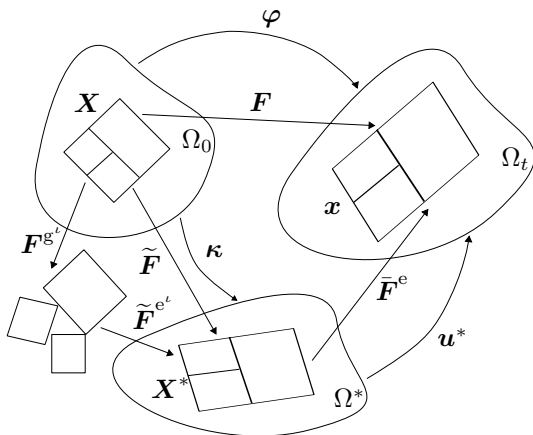
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Growth kinematics



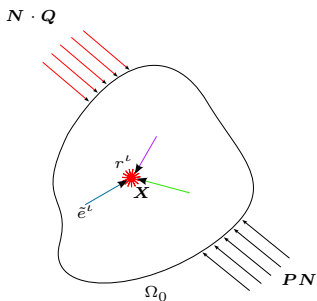
- $F = \bar{F}^e \tilde{F}^{e^t} F^{g^t}$; $F^{e^t} = \bar{F}^e \tilde{F}^{e^t}$; Internal stress due to \tilde{F}^{e^t}
- Isotropic swelling due to growth: $F^{g^t} = \frac{\rho_0}{\rho_{0_{int}}} 1$
- Saturation and swelling

Growth kinematics



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Energy balance and entropy inequality



- ρ_0^ℓ – Species concentration
- e^ℓ – Specific internal energy
- P^ℓ – Partial stress
- F – Deformation gradient
- V^ℓ – Species relative velocity
- Q^ℓ – Partial heat flux
- r^ℓ – Species heat supply
- \tilde{e}^ℓ – Energy transfer
- M^ℓ – Species flux

$$\rho_0^\ell \frac{\partial e^\ell}{\partial t} = P^\ell : \dot{F} + P^\ell : \nabla_X V^\ell - \nabla_X \cdot Q^\ell + r^\ell + \rho_0^\ell \tilde{e}^\ell - \nabla_X e^\ell \cdot (M^\ell)$$

Constitutive relations for fluxes

- Combine first and second laws to get dissipation inequality
- Constitutive hypothesis $e^l = \hat{e}^l(\mathbf{F}^{e^l}, \rho_0^l, \eta^l)$
⇒ Consistent constitutive relations

- Fluid flux relative to collagen

$$\mathbf{M}^f = \mathbf{D}^f \left(\rho_0^f \mathbf{F}^{T^f} \mathbf{g} + \mathbf{F}^{T^f} \nabla_{\mathbf{X}} \cdot \mathbf{P}^f - \nabla_{\mathbf{X}} (e^f - \theta \eta^f) \right)$$

- Solute flux (proteins, sugars, nutrients, ...) relative to fluid

$$\tilde{\mathbf{V}}^s = \mathbf{V}^s - \mathbf{V}^f$$

$$\tilde{\mathbf{M}}^s = \mathbf{D}^s \left(-\nabla_{\mathbf{X}} (e^s - \theta \eta^s) \right)$$

- \mathbf{D}^f and \mathbf{D}^s – Positive semi-definite mobility tensors
Magnitudes from literature, e.g. Mauck et al. [2003]

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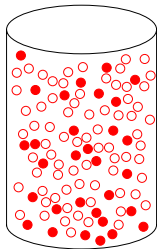
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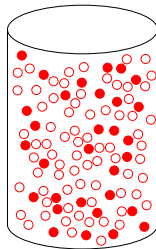
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Saturation and Fickian diffusion



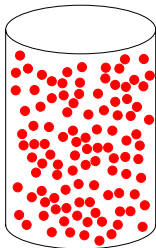
Configuration 1



Configuration 2

- Change in configurational entropy with distribution of solute particles ... **if** solvent is not saturated with solute

Saturation and Fickian diffusion



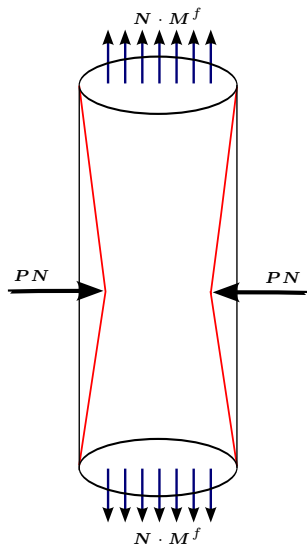
Only possible configuration

- Saturated \Rightarrow Single configuration \Rightarrow No Fickian diffusion
- Still have concentration-gradient driven transport due to stress gradient contribution to flux

Computational formulation details

- Implementation in FEAP
- Coupled implementation; Staggered scheme (Armero [1999], Garikipati et al. [2001])
- Nonlinear projection methods to treat incompressibility (Simo et al. [1985])
- Energy-momentum conserving algorithm for dynamics (Simo & Tarnow [1992a,b])
- Backward Euler for time-dependent mass balance
- Mixed method for stress/strain gradient-driven fluxes (Garikipati et al. [2001])
- Large advective terms require stabilization

Examples of coupled computation – Constriction



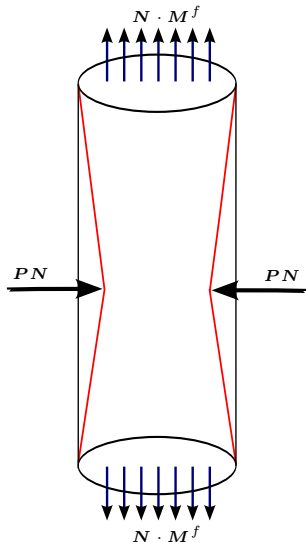
- Simulating a tendon immersed in a bath
- Constrict it to force fluid and dissolved nutrient flow \Rightarrow guided tendon growth
- Biphasic model

• Fluid mobility $D_{ij}^f = 1 \times 10^{-8} \delta_{ij}$,
Han et al. [2000]

- First order rate law:

$$\Pi^f = -k^f(\rho^f - \rho_{0,im}^f), \quad \Pi^c = -\Pi^f$$

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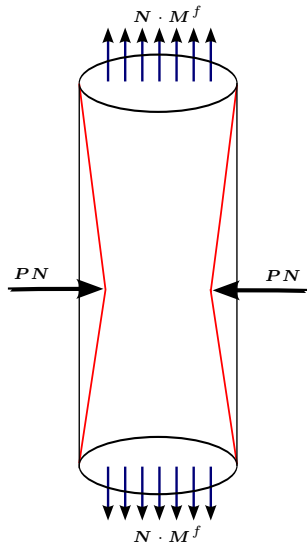


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Results and inferences

- Total flux in the vertical direction
- Stress driven diffusion

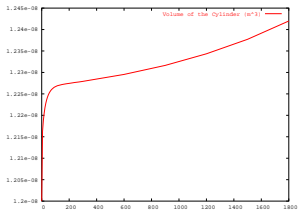
Results and inferences

- Regions of high fluid concentration
⇒ Faster growth
- Relaxation after constriction concludes

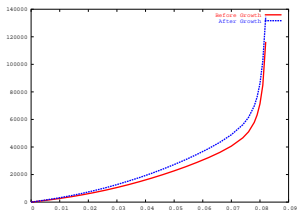
Swelling of a tendon immersed in a bath

Collagen concentration evolution

Volume evolution curve



Stress-extension curves



Summary and further work

- Physiologically relevant continuum formulation describing growth in an open system – consistent with mixture theory
- Relevant driving forces arise from thermodynamics – coupling with mechanics
- Gained insights into the problem
 - Issues of saturation and growth
 - Saturation and Fickian diffusion
 - Configurations and physical boundary conditions
- More careful treatment of biochemistry – nature of sources
- Formulated a theoretical framework for remodelling
- Engineering and characterization of growing, functional biological tissue to drive and validate modelling

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